

# Preprocessing MRI Images of Colorectal Cancer

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## Abstract

The precision cancer diagnosis is possible owing to the sophisticated technologies based digital image processing tools. Among the various imaging modalities, Magnetic Resonance Imaging (MRI) is of paramount interest, especially for colorectal cancer imaging. Despite the fact that MRI is a superior technology, an MRI image does contain artifacts and distorted signals. Numerous algorithms and approaches have been studied and implemented for various cancer diagnostics. Yet, more augmented techniques need to be developed, since the study is complex and needs a maximum possible accuracy of detection. In this paper, the research work focuses on the various preprocessing techniques such as noise removal techniques and image enhancement techniques. These methods are analyzed for their performance using statistical parameters and the optimal method is determined for generating a noise-free edge-sharp intensity enhanced MRI images of colon and rectum cancer, paving for precision diagnosis. The experimental results are analyzed in terms of various image quality metrics.

**Keywords:** *Preprocessing, colorectal cancer, contrast enhancement, sharpening, denoising, filtering, image quality metrics.*

## 1. Introduction

The design of computer-assisted medical diagnostics, especially for early detection of various types of cancer in patients, involves extensive application of digital image processing techniques. Though many techniques have been developed for automated cancer diagnosis, still it is niche area due to the higher accuracy level expected of these systems. Colorectal cancer is the third biggest threat worldwide and it requires superior automated tools for its early detection and

subsequent treatment plan. The main modalities of medical imaging of colon and rectum region are CT, PET, MRI and X-Ray. The digital images acquired through such modalities are prone to noise and possibilities of artifacts, which may be due to the modality itself or due to the particles present in the environment between the imaging device and the scanned human body. The presence of such artifacts may lead to an improper diagnosis of the diseases. This is because the features extracted from the regions of interest (ROI) do not represent the lesion more precisely and thus fail to detect the existence of malignity. Thus it is imperative to have effective preprocessing step for treating such images for noise removal and image enhancement. To have a more justification on the need of preprocessing, one has to look into the details of image acquisition. In any imaging modality, whether CT, PET or MRI, the images normally consist of artifacts which may be due to one of the following reasons: patient-specific artifacts which occur due to metal artifacts, hardening of motion beam; the processing method and equipment based artifacts are usually caused due to partial volume effect, ring and staircase [1]. Hence, it is essential that these images undergo preprocessing operations before being considered for diagnosis.

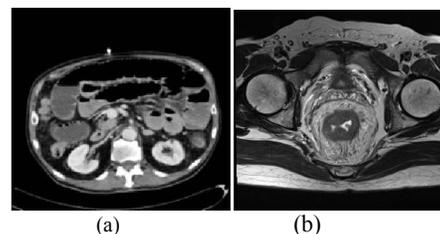


Fig 1: Blurred and noisy MRI images of (a) colon and (b) rectum cancer (Courtesy : Radiopaedia)

Figure 1 shows a colon and a rectum MRI image which are noisy and blurred. With this image quality, it will be difficult for an automated system to draw inference. Several research efforts that address this issue have been reported in the literature survey for removing the noises, artifacts and enhancing the brightness and contrast of images of modalities like CT, X-RAY as well as MRI for various types of medical images. In this, the objective is to develop a better method of noise and artifacts removal and thus achieve image enhancement of MRI images of colon and rectum cancer.

## 2. Concepts of Preprocessing

In digital image processing, preprocessing of an image involves low level processes such as noise reduction, image enhancement, image sharpening, etc. [1]. Image enhancement is achieved in terms of improving the sharpness, brightness, contrast (if required) by de blurring the image, removing the noise and transforming the colour, hue and intensity levels and, thereby making the image better suited for the application under consideration[2]. When an image is acquired by an imaging device through some modality, the immediate process required is scaling. In particular, the medical images are acquired through modalities like MRI, CT, Colonoscopy, PET, etc. After scaling, the image preprocessing needs to be performed to improve the clarity of the image that facilitates image analysis.

Contrast enhancement is preferred for MRI images, since it is not a color image. Three contrast enhancement techniques, namely, general contrast enhancement, histogram equalization, adaptive histogram equalization, are in popular use. The general contrast adjustments technique maps the intensity values in the input grayscale image with that of the specified values; if low and high values are not specified, then 1% of data is saturated at low and high intensities of the image. Thus it increases the contrast of the output image. In histogram equalization, the contrast is enhanced by redistribution of pixel values with uniform probability distribution.

In adaptive histogram equalization, the grayscale image is transformed using contrast-limited adaptive histogram equalization (CLAHE). The difference between histogram equalization and adaptive histogram equalization is that in the second one the CLAHE works on small regions in

the image may be in tiles or cells, rather than the entire image. So each cell's contrast is enhanced. In order to avoid induced boundaries, the neighboring tiles are then joined using bilinear interpolation.

The contrast enhanced image is further sharpened using high pass filter, which is a frequency domain filter. It is used for sharpening the edges of the image and, at the same time, preserving the information. Next issue to be addressed is noise removal. The reason for noise in the image is either due to acquisition modalities or later when the image gets transmitted. Thus the model of a noisy image can be given as:

$$Z(x,y) = X(x,y) + Y(x,y) \quad (1)$$

In Eq.(1),  $X(x,y)$  is the original image,  $Y(x,y)$  represents the noise in that image and  $Z(x,y)$  is the resultant noisy image. Noise removal techniques can be broadly divided into approaches based on filtering, wavelet and multifractal. The different noise models are salt and pepper noise, Gaussian noise, Poisson noise and Speckle noise [3]. Since it is difficult to decide by perception, the type of noise in an image, the selection of a particular noise model and the respective denoising technique is purely based on the type of image and its application. There is no generalized approach that can be followed for all type of images and all types of applications. Hence, these methods are required to be tested in order to find the suitable technique for the type of image modality considered for disease diagnostics under study. The nature of different noise types is given below:

### 2.1 Salt and Pepper Noise

It is seen as white and black pixels sparsely. It appears as spots in and around the image. It is generally used as a model to detect the defects in the images during transmission.

### 2.2 Gaussian Noise

Gaussian noise, or random noise, is based on statistics having a probability density function (PDF) as that of Gaussian distribution.

### 2.3 Poisson Noise

This noise, also known as photon noise, has a form of uncertainty when measuring light with respect to photon detections. In bright light, its expected magnitude is dependent on the signal and becomes

dominant in the image. This is a form of shot noise which follows Poisson distribution.

## 2.4 Speckle Noise

This noise is granular in nature and inherently exists in all types of images taken through various modalities and sources. It degrades the quality of images very apparently and the information is lost.

The filtering techniques, namely, mean filter, median filter and adaptive median filters, are prominently used for denoising medical images. In the mean filter, also known as average filter, a 3x3 window is used to replace the central pixel value by the average of the nine pixels of the window. It basically helps in reducing the noise and smoothen the image. In the median filter, a 3x3 window is used to replace the central pixel value by the median of the nine pixels of the window. It removes noise. Further, it overcomes the reduction of image sharpness of mean filter and, hence, suitable for edge detection or region growing. The adaptive median filter can handle both impulse and non impulse noise. Besides smoothening, it also preserves the details of the image. Instead of replacing the centre pixel with the median value, this filter replaces corrupted (noisy) pixels in the window by the median value of the pixels in the filtering window. Adaptive median filter is best suited for low noise densities because those corrupted pixels which undergo replacement are very few. At higher noise densities, the window size has to be increased so that a better noise removal can be achieved.

In this paper, the objective is to investigate preprocessing methods for image enhancement of MRI images of colon and rectum that improve image quality and thus assist digital image analysis based cancer diagnostics. The contrast adjustment, sharpening and noise removal are considered. Different noise models are explored and the statistical parameters of image quality are evaluated to find the optimal method of denoising such images.

## 3. Related Work

There are numerous preprocessing techniques for digital image processing. The most important among those techniques are image enhancement and denoising. In medical imaging applications, image denoising plays a vital role. Despite high technology medical imaging modalities, the need

for preprocessing these images persists before any image analysis is undertaken.

### 3.1 Noise Removal and Filters

An efficient noise reduction algorithm proposed for CT images in [4] uses window-based multi-wavelet transformation and thresholding for Gaussian noise removal and image enhancement. Neha et al.[5] bring out the comparative results of various filtering techniques applied on MRI images of brain cancer, which show that max filter performs better than mean, arithmetic mean and min filters. Valarmathy et al. [6] have examined mean, median and adaptive median filters for removal of noise. Geetha and Selvi[7] have done comparative analysis of various denoising methods in terms of peak signal to noise ratio (PSNR), signal to noise ratio (SNR) and validated by visual inspection of the images. In the absence of prior knowledge of the type of noise existing in an image, most research efforts aim for removal of Gaussian noise and often do not give required results. Discrete wavelet transformation algorithms are also developed in the literature for image denoising.

Priyadarshini[8] has proposed a new denoising technique for MRI images of brain which is based on spectral subtraction method. Signal to noise ratio (SNR) has been improved significantly by the proposed technique. The filter referred as SSD(Spectral Subtraction Denoising) is a filter mainly dependent on the SNR value. Here, the lower SNR components have reduced the virulence than higher SNR components. Wavelet denoising method is used by JecilyJemila and Jayshankar [9], which has enhanced the visual quality of images. This improvement leads to the accuracy of image segmentation. In case of functional MRI, wavelet based denoising methods help in increasing the SNR level, which retains the shape of the region of interest. Rajesh Patil and Bhalachandra [10], have used high pass filter and median filter for noise removal and enhancement, which led to effective brain tumor extraction. It has also used water shed segmentation and threshold segmentation for extracting the brain tumour region. Usage of filters have resulted in good quality, enhanced image of the brain. Siti et. al [11], have used an algorithm for denoising the noisy MRI images, termed as switching AFKM, is proposed for segmentation process and then a conventional clustering algorithm is used for clustering the objects. The

proposed method minimizes the salt and pepper noise and sharpens the image, thus giving a good quality image output.

Gopinath[12] presented the high pass filter for enhancement of the MRI image of prostate cancer and has used median filter for removing noise. Anuradha et al. [13] have used median filter for removing the salt and pepper noise. Ben George and Karnan[14] proposed a method for preprocessing of MRI image of brain. After comparing median filter, weighted median filter and center weighted median filter, it was found that center weighted median filter yields optimal results for noise removal and image enhancement. Deepa and Sumithra[15] have proposed a different technique which combines the spectral subtraction and wavelet packet based methods. This method has been used to test for the common four types of noises at various decibel levels. The result has shown that it has not only removed the noise but also has maintained the image quality. Deepa and Suganthi [16], have done a performance evaluation of various filters for denoising medical images. A study of noise detection and noise removal techniques for medical images has been done by Bhausaheb et. al. [17], which reveals that the choice of noise inputs and the relevant noise removal filters in medical images, such as MRI, CT Scan, X-ray, depends on the type of noise existing in these images on acquisition and so a general technique cannot be used for noise input and removal. Amutha et al. [18] have presented a spatially adaptive method, namely, optimized single-stage principal component analysis (OSPCA) for improving the signal to noise ratio in MRI images of breast. The information and the clarity of image can't be distorted while using denoising filters. So to protect the data, blocks of similar pixels are grouped together using local pixel grouping (LPG) and the image is transformed in PCA domain. When smoothing is done, shrinking techniques is used so that the information is preserved.

### 3.2 Contrast enhancement

Oak and Kamathe [19] have presented a histogram based approach for contrast enhancement and observed that, for T1 weighted axial images of brain MRI, modified bi-histogram equalization(BHE) and contrast limited adaptive histogram equalization (CLAHE) give good

contrast but still has some disturbed background. Brightness preserving bi-histogram equalization (BBHE) gives good contrast for the same. Similarly, for T2 weighted axial MRI images, CLAHE and BBHE are much more suitable. However, BBHE gives uniform histogram and CLAHE gives clipped histogram. For proton density (PD) weighted images, BBHE or modified BHE is seen to be the optimal option. Reddy et al. [20] proposed a methodology for detecting the bone cancer by identifying the mean intensity of MRI image. Once malignity is detected based on mean intensity threshold value, the stage of the cancer is also identified. Further, it focuses on detecting the cancer based on tumor size in an MRI image and cancer stage based on mean intensity threshold value.

Nelinkanti et al. [21] proposed a framework to enhance the input MRI image with various image processing techniques and used adaptive k-means clustering technique for segmentation. This segmented image is further analyzed for detecting the presence of colorectal cancer. The calculation of area, mean of the tumor and the minimum distance from tumor to other parts will assist radiologists in finding the stage further. Some researchers have focused on operations other than preprocessing. A new method has been introduced by Harish Kumar et al. [22] for enhancement of mammographic images, which is based on modified mathematical morphology and bi-orthogonal wavelet transform. The performance of this method is evaluated using contrast improvement index (CII) and edge preservation index (EPI). The results show that the proposed method is better in giving good quality image. Modified tracking algorithm is used by Velusamy et al. [23] for removing the artifacts present in the acquired brain MRI image. This algorithm uses the threshold value of the artifact to remove the disturbances. The filtering technique used here is the centre weighted median filter. Niu et al. [24] have used 2D wavelet packet transform, as a preprocessing method and found it to be more effective in spectral data compression and feature extraction. Histopathological image analysis using image processing techniques has been investigated by Belsare et al.[25], and no specific method is proposed for preprocessing.

KimmiVerma et al. [27] have compared various image preprocessing and segmentation algorithms

and the choice of the techniques varies according to the type of image acquired. Apart from noise removal, Deshpande et al. [13] have done contrast enhancement of the image. In [27], linear-filtering technique is used by Atiyeh Hashemi and et.al., for enhancing the CT mages of lung cancer. Sheela and Suresh Babu [28] have used skull stripping and histogram equalization for preprocessing the brain MRI images and obtained satisfactory results.

#### 4. Methodology

The proposed methodology for preprocessing MRI images of colon and rectum cancer is depicted in the Figure 2 and comprises the following steps:

- i. The input MRI images of colon and rectum cancer are converted into gray scale images, which are subjected to contrast enhancement. The image enhancement is measured in terms of statistical parameters of image quality, namely, AMBE, Structural Similarity Index (SSIM), FSIM, Peak to Signal Noise Ratio (PSNR), Mean Square Error (MSE), Signal to Noise Ratio(SNR), CNR.
- ii. Image sharpening is performed on the contrast enhanced images using high pass filter.
- iii. Noise content is added to the input MRI image and then removed with various filtering techniques. Different proportions of noise, which are modeled as salt-and-pepper, Gaussian, Poisson and speckle noise, are considered.
- iv. The noise removal is done using the mean, median and adaptive median filters. The optimal filter is determined based on Mean Square Error (MSE) and Peak to Signal Noise Ratio (PSNR).

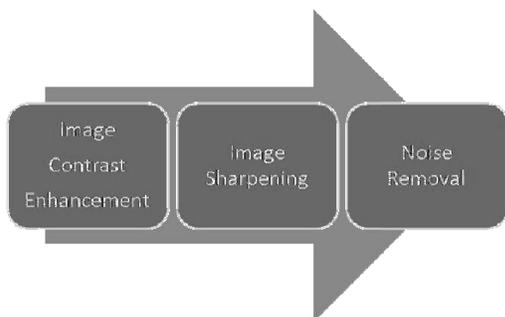


Fig. 2 Block Diagram of the Preprocessing Methodology

The Table 1 describes the various performance metrics along with the degree, wherein L indicates that the value should be low and H indicates the value should be high. The optimal t

technique at each step is chosen based on these metrics levels.

Table 1: Image Quality Metrics

Metrics	Description	Formula	Degree
MSE	MSE is the square of difference between original and reconstructed image.	$MSE = \frac{1}{mn} \sum_{i=0}^n \sum_{j=0}^{n-1} \ f(i,j) - g(i,j)\ ^2$	L
SNR	Signal to Noise Ratio is the ratio of the power of signal of the original image to that of the power of signal of noisy image or reconstructed image. Some times it is represented as the mean of both signals. While calculating power, SNR is represented in decibels, where as in mean ratio it is represented as a number.	$SNR = \frac{P_{signal}}{P_{noise}} = \frac{\mu}{\sigma}$	H
CNR	Carrier-to-Noise Ratio is the ratio of the power of the modulated signal to the power of the noise found in the information signal after it has been demodulated. Here it is power of the original image signal and power of the reconstructed image signal.	$CNR = \frac{ABS(S_f - S_g)}{\sigma}$	H
PSNR	Peak Signal to Noise Ratio. This metric is used to measure the quality with that of the original or corrupted image. It is a logarithmic (dB) scale which is the maximum value of maximum signal power.	$PSNR = 20 \log_{10} \left( \frac{MAX_f}{\sqrt{MSE}} \right)$ <p>f = original image                      MSE is as calculated above in point 1                      MAX<sub>f</sub> is the maximum signal value of the original image</p>	H
SSIM	Structural Similarity Index Measure is a method for measuring the similarity between the original image and reconstructed	$SSIM(X,Y) = \frac{(2\mu_x\mu_y + C_1)(2\sigma_{xy} + C_2)}{(\mu_x^2 + \mu_y^2 + C_1)(\sigma_x^2 + \sigma_y^2 + C_2)}$	H

	image. Here the original image is considered as perfect and the reconstructed image is compared with it		
FSIM	Feature Similarity Index Measure is a measure which looks at the feature parameters involved in the images and compares for a match and high quality of intensity values.	$FSIM = \frac{\sum_{x \in \Omega} S_L(x) \cdot PC_m(x)}{\sum_{x \in \Omega} PC_m(x)}$	H
RFSIM	Riesz-transform based Feature SIMilarity index. It is computed by comparing the feature maps at key locations marked by a feature mask between two images.	$RFSIM = \prod_{i=1}^5 D_i$ <p>where</p> $D_i = \frac{\sum \sum d_i(x,y) \cdot M(x,y)}{\sum \sum M(x,y)}$	H
UQM	Universal Quality Measurement	$Q = \frac{1}{M} \sum_{j=1}^M Q_j$	H
IFC	Information Fidelity Criterion is used to evaluate how much information are same in original image and reconstructed image	$IFC = \sum_{k \in \Omega} I(C^{N_i,k}; D^{N_i,k}   S^{N_i,k})$	H
MAE	Mean Absolute Error is the mean or average of absolute difference between the original image and image after reconstruction	$AVG(abs(f-g))$	L
AMBE	Absolute Mean Brightness Error is used to calculate the absolute value of the difference between the mean error original image and mean error of reconstructed image	$ABS(AVG(MAE1 - AVG(MAE2)))$	L

## 5. Experimental Results

The experimentation of the proposed methodology

is carried out on the image data set consisting of MRI images of colon and rectum of 15 patients, both being the axial T2 weighted images obtained from MRI scan, using MATLAB software. Thus, the dataset contains 30 MRI images (15 colon and 15 rectum images), which have a combination of normal and abnormal tumours varying from the stage T1 to T4.

Since the original MRI image is already in black and white format, not much of variation is seen on grayscale conversion. But the images are converted to 8 bit format so that it is easy to process at the low level. The Figures 3(a)-(d) show a sample colon image and its corresponding resultant images obtained by contrast enhancement methods, namely, general contrast, histogram equalization and adaptive histogram equalization. The Figures 4(a)-(d) show a sample rectum image and its corresponding resultant images. The results are compared in terms of the image quality metrics. PSNR value is very high compared to other parameters.

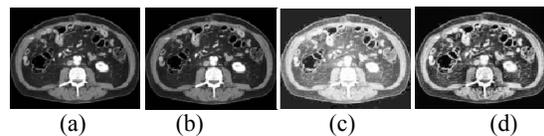


Fig 3 Colon image: (a) Original image (b) Contrast general (c) Histogram equalization (d) Adaptive histogram equalization.

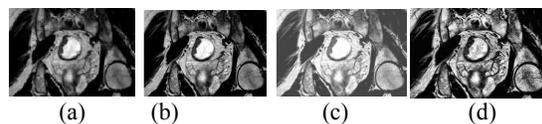


Fig 4 Rectum image: (a) Original image (b) Contrast general (c) Histogram equalization (d) Adaptive histogram equalization.

By visual inspection, the adaptive histogram equalization yields better image enhancement results. However, image quality needs to be analyzed in terms of some statistical parameters. There are various methods available to evaluate the image quality attained by an image processing technique, which are classified as full reference methods (FR) and no reference methods (NR). The FR methods use a reference image for comparison with the newer image achieved through some process. The NR methods on the contrary do not have any reference image to compare. Usually in image enhancement, the FR methods are used so that the resultant image is evaluated to be better or not. The factors used for such reference are

sharpness, brightness, contrast, colour, noise, artifacts and distortion. In this paper, FR methods are used for performance evaluation [3] and most of the evaluation parameters mentioned in the Table 1 are computed for images obtained by the three image enhancement methods, namely, contrast adjustment, histogram equalization and adaptive histogram equalization.

The experimental results are presented in the Table 2 for colon and rectum images. It is observed that contrast adjustment method yields higher values for PSNR, SSIM, FSIM, RFSIM, UQM and lower value for AMBE, as compared to the other two methods. Since the contrast adjustment performs better in terms of majority of the metrics, it is a suitable method for image enhancement of MRI images of colon as well as rectum.

Table 2 Comparison of image quality metrics of colon and rectum MRI images obtained by different contrast enhancement techniques-IQM(Image Quality Metrics), CA(Contrast Adjustment), H(Histogram), AH(Adaptive Histogram)

IQM	Colon Images			Rectal Images		
	CA	H	AH	CA	H	AH
SNR	-0.003	-2.37	-0.549	-0.067	-1.083	-0.475
CNR	37.228	49.58	55.936	46.252	54.476	60.575
AMBE	1.0443	67.85	15.329	15.234	69.729	34.476
SSIM	0.997	0.388	0.523	0.929	0.498	0.537
PSNR	30609.32	11.325	19.660	26225.7	10.552	15.122
RFSIM	0.993	0.250	0.268	0.849	0.297	0.120
MAE	0	0.161	1.857	0.006	0.005	0.718
UQM	0.999	0.433	0.656	0.928	0.483	0.616
IFC	3.57E-06	3.57E-06	3.57E-06	1.87E-06	1.87E-06	1.87E-06
FSIM	0.999	0.841	0.889	0.972	0.863	0.827

The Figures 5a and 5b shows the comparison of the image quality metrics computed for colon and rectum MRI images using the three types of contrast enhancement techniques and the metric values are the mean of the values obtained for all the colon/rectum images.

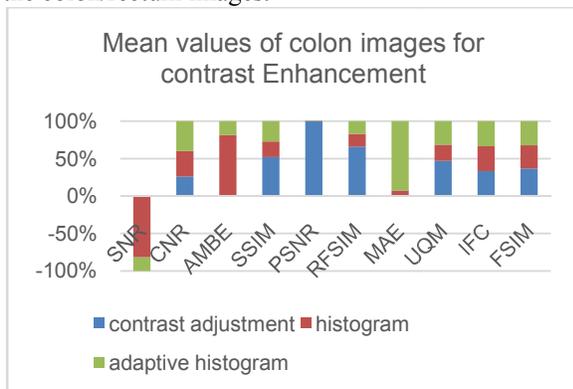


Fig 5a : Comparison of image quality metrics of colon MRI images using the three types of contrast enhancement techniques.

Except CNR, all high degree metrics have higher values yielded by contrast adjustment.

From the Figure 5a and 5b, it is clear that contrast adjustment performs better than the other two methods for most of the parameters.

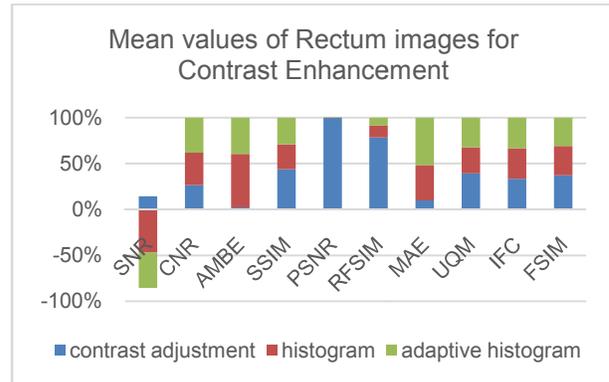


Fig 5b : Comparison of image quality metrics of rectum MRI images using the three types of contrast enhancement techniques.

Next, the contrast adjusted images are subjected to image sharpening using high pass filter. The Figure 6 shows samples of one colon image and one rectum image with resultant images obtained by the contrast adjustment followed by sharpening.

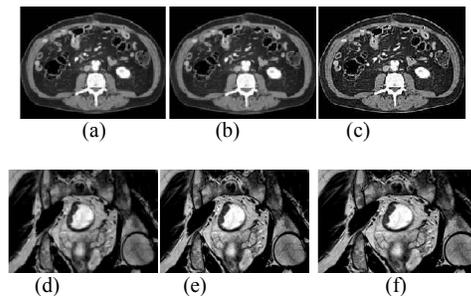


Fig 6 : Image sharpening: (a) and (d) Original MRI images of colon and rectum; (b) and (e) Contrast enhanced images of colon and rectum in (a) and (d); (c) and (f) Sharpened images of colon and rectum in (b) and (e).

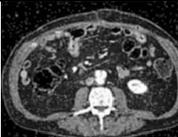
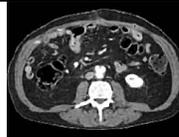
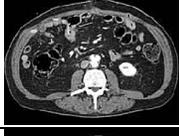
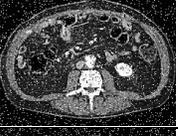
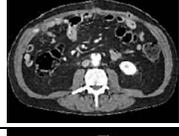
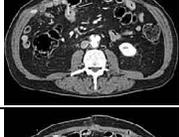
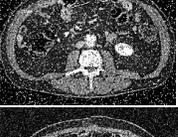
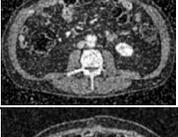
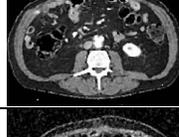
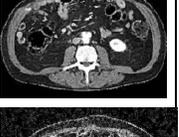
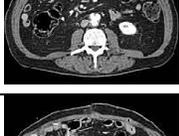
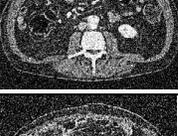
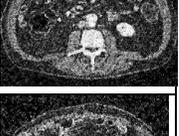
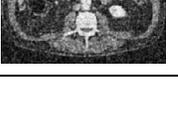
Finally, the sharpened images are subjected to image denoising process. The four noise models, which are in popular use [3][6][9][12], namely, salt-and-pepper(SP), Gaussian (GN), Poisson (PN) and speckle (SK) noise, are considered. The three noise removal filters, namely, mean(MF), median(MDF) and adaptive median(AMDF) filters, are employed and their performance is studied in terms of MSE and PSNR metrics, which are the

most preferred measures of image quality after noise removal. For salt and pepper, Gaussian and speckle noise, the noise proportions are varied as 5%, 10% and 15% and then tested with the three filters to remove the added noise along with the inherent noise of that type in the image. In case of Poisson noise, the tool takes the proportion itself within the intensity of the image, and hence specific proportion is not mentioned. The Figure 7 shows the resultant images of denoising by the three filters applied on a sample colon MRI image, while the Figure 8 shows that on a sample rectum MRI image. The experiment is repeated for all the 15 images of colon and 15 images of rectum. While analyzing the metrics, the mean values of MSE and PSNR taken over all the 15 images are considered for each of the noise model, proportion and filter applied.

In order to find the optimal filtering, the peak signal to noise ratio (PSNR) and mean square error (MSE) values of the denoised images are calculated. The PSNR value should be high and MSE value should be low for optimal filtering.

The Table 3 gives the PSNR and MSE values obtained for colon and rectum MRI images using the different noise types with various proportions and noise filters. It is observed that, for colon images with salt and pepper noise, the adaptive median filter yields the highest PSNR and lowest MSE values.

For rectum images with Poisson noise, the mean filter yields the lowest MSE, whereas for that with salt and pepper noise, the adaptive median filter yields highest PSNR value. However, the difference of MSE values corresponding to salt and pepper noise and Poisson noise for rectum image is 0.00173, which is marginal. Thus, the adaptive median filter can be considered as optimal for rectum images also. Similarly, the optimal filters suitable for removing other noise types are determined and presented in the Table 4.

Sharpened Image	Noise Type	Added Noise Proportion	Noisy Image	Denoised image		
				Mean filter	Median filter	Adaptive Median filter
	Salt and Pepper (SP)	5%				
	Salt and Pepper (SP)	10%				
	Salt and Pepper (SP)	15%				
	Gaussian (GN)	5%				
	Gaussian (GN)	10%				

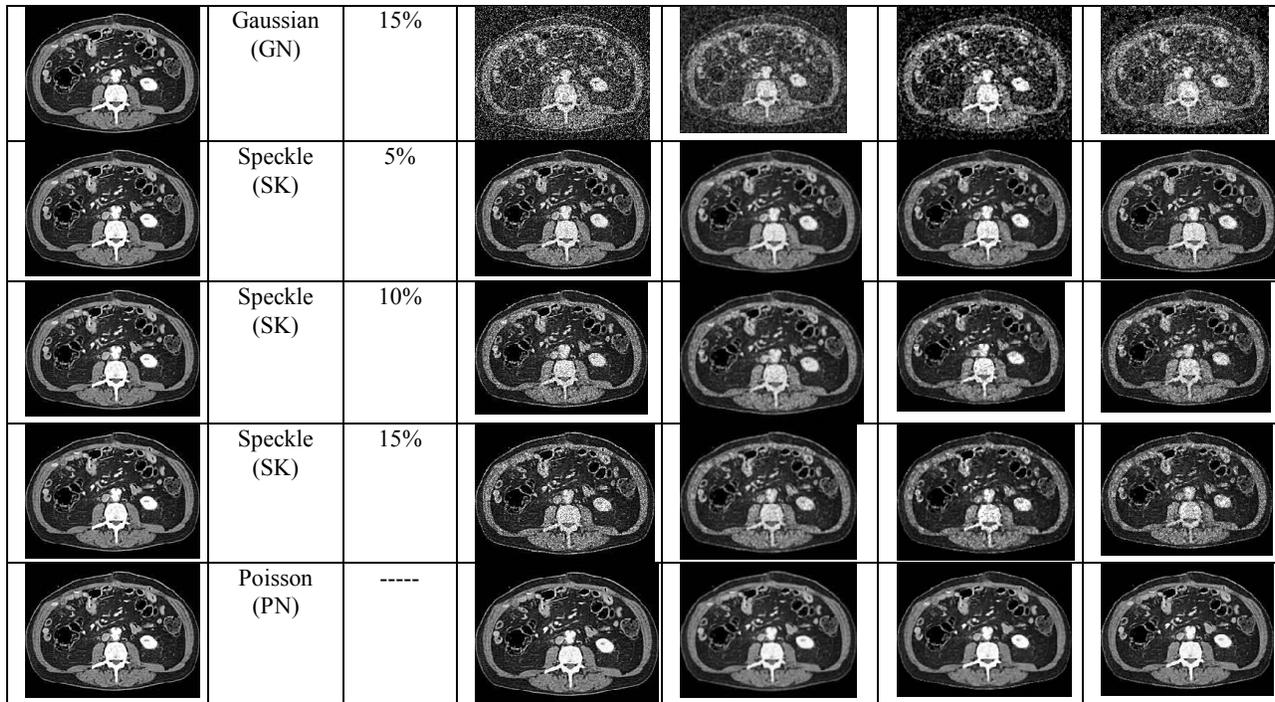
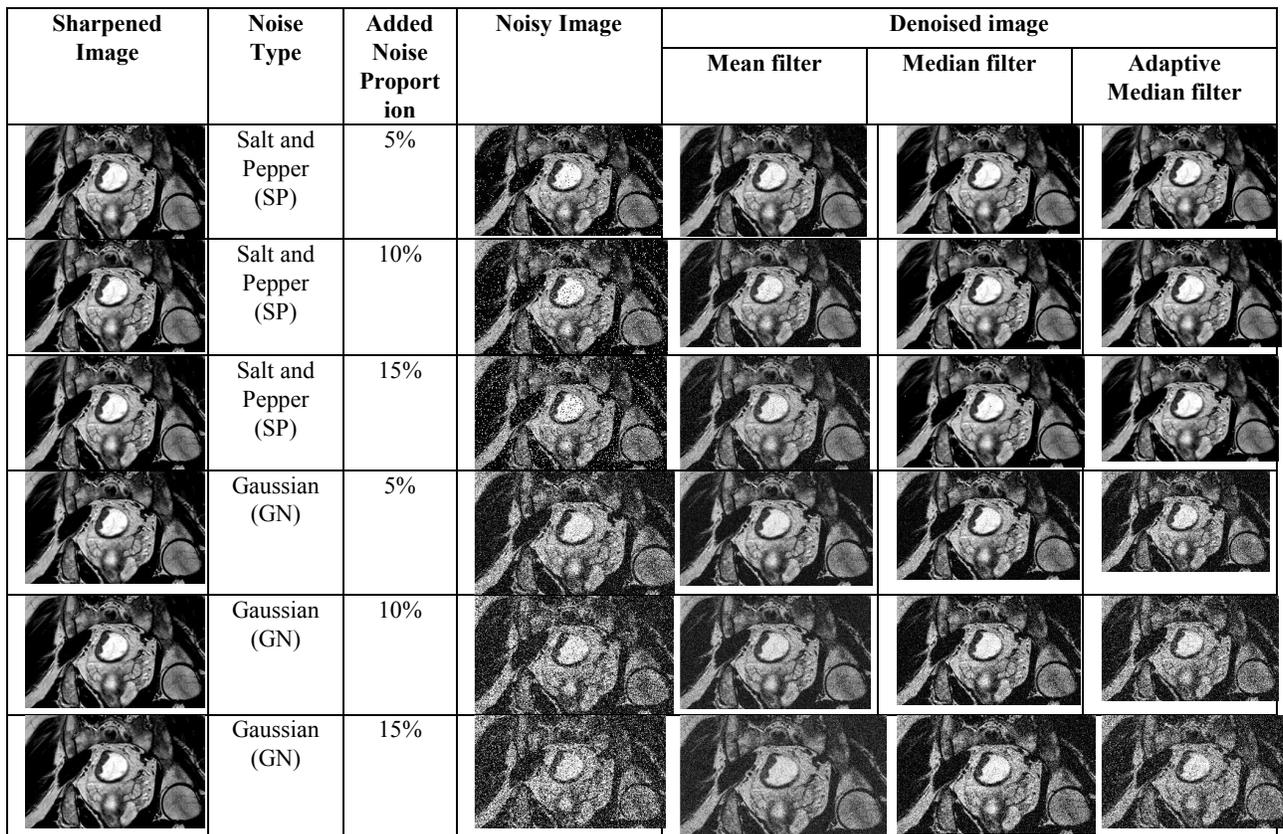


Fig 7 Sharpened image of a sample colon MRI image and corresponding denoised images obtained by using mean, median and adaptive median filters for different noise types and proportions.



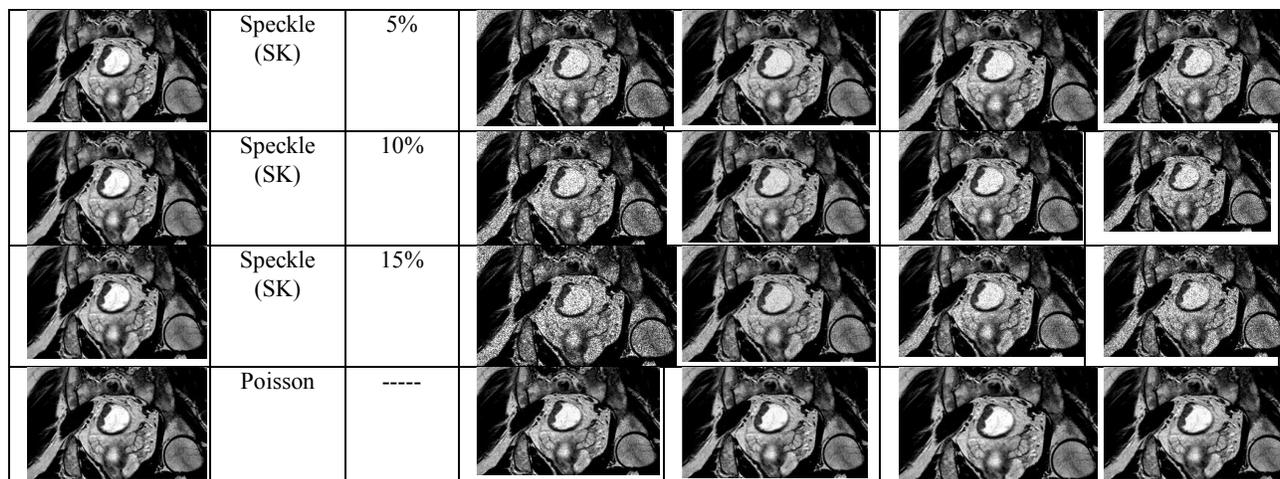


Fig 8 Sharpened image of a sample rectum MRI image and corresponding denoised images obtained by using mean, median and adaptive median filters for different noise types and proportions.

Table 3 : Performance comparison of noise filters in terms of MSE and PSNR values of denoised images colon and rectum for different noise types and proportions-Noise Model(NM), Noise Proportion(NP), Filtering Method(FM).

NM	NP (%)	FM	Colon Images		Rectal Images	
			PSNR	MSE	PSNR	MSE
SP	5	MF	24.64781	0.003662	23.53642	0.006587
SP	5	MDF	34.1166	0.000727	32.64571	0.006856
SP	5	ADMF	<b>38.18087</b>	<b>0.000309</b>	<b>36.10664</b>	0.006154
SP	10	MF	21.75163	0.006865	21.07674	0.009371
SP	10	MDF	32.66881	0.000928	31.06208	0.006956
SP	10	ADMF	36.7396	0.00041	34.85967	0.006171
SP	15	MF	19.80499	0.010624	19.42707	0.012679
SP	15	MDF	30.49571	0.001289	28.67322	0.007192
SP	15	ADMF	35.24684	0.000528	33.66746	0.006203
GN	5	MF	20.78644	0.008466	20.45601	0.010335
GN	5	MDF	21.4844	0.007242	19.83983	0.012229
GN	5	ADMF	17.5263	0.017747	16.94425	0.020635
GN	10	MF	18.15007	0.015433	18.15962	0.016204
GN	10	MDF	18.8182	0.01325	17.67728	0.018211
GN	10	ADMF	14.96653	0.031923	14.62416	0.034756
GN	15	MF	16.62497	0.021915	16.7846	0.021739
GN	15	MDF	17.22685	0.019068	16.34384	0.024048
GN	15	ADMF	13.58839	0.043806	13.33766	0.046598
SK	5	MF	27.3768	0.002257	25.45608	0.005265
SK	5	MDF	26.50544	0.002496	23.16845	0.008411
SK	5	ADMF	23.72444	0.004538	21.01868	0.010007
SK	10	MF	25.36213	0.003395	23.54946	0.006264
SK	10	MDF	24.05114	0.004296	21.24749	0.010135
SK	10	ADMF	21.02295	0.008469	19.02555	0.013802
SK	15	MF	24.02092	0.004528	22.36101	0.007282
SK	15	MDF	22.53785	0.006047	20.09648	0.011853
SK	15	ADMF	19.42026	0.012272	17.81784	0.017458
PN	--	MF	31.03802	0.003393	29.72008	<b>0.004424</b>
PN	--	MDF	32.37568	0.00428	28.91812	0.006963
PN	--	ADMF	31.30535	0.008426	26.86018	0.006589

Table 4 : The optimal noise filters for different noise models

Noise model	Filtering method	
	Colon image	Rectum image
SP	ADMF	ADMF
GN	MDF	MF
SK	MF	MF
PN	MDF	MF

## 6. Conclusion

In this paper, the preprocessing of MRI images of colon and rectum is investigated by considering various methods of digital image enhancement, image sharpening and image denoising. The suitable methods that yield optimal results in terms of different image quality metrics are determined. The experimentation has been carried out on the MRI images of colon and rectum showing incidence of various stages of cancer. It is observed that contrast adjustment technique for image enhancement, which is further sharpened using high pass filtering, yields good quality image. Further, the noise filters, namely, mean, median and adaptive median filters, are employed to denoise the sharpened image and obtain better quality image. The proposed preprocessing yields a clear image without any artifacts and at the same time without loss of any information. The outcome of the present investigation is helpful in assisting precision diagnosis of abnormality or finding the stage of colorectal cancer.

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